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## "KERATOMETRIC MODULE FOR COUPLING TO SLIT LAMPS AND OR OCULAR MICROSCOPES.

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The present invention refers to an ophthalmic device, for coupling in Slit Lamps or Ocular Microscopes, with the purpose of utilizing the image to selectively measure the cornea's curvature and examine its topography under the examination mode of the instrument in reference, which is composed by an illuminated ring or projection mask and a device to observe the reflected image from the surface where the ring is projected onto. The mask, coupled onto the objective lens or any fore part of the Slit Lamp, in projection axis A, allows the passage of light through axes A and B, and thus the reflected image from the patient's cornea or reflecting surface, through its central holes. The ring or mask allows the illuminated ring's or mask's image to be centered by the cornea or reflecting surface by a fixation point for the patient's eye, which must be aligned with the respective light ring and the system's optical axis. The alignment with the fixation point allows the passage of the ring's image reflected from the eye, through the center of the objective lens of the slit lamp, and by means of mechanical alignment of the patient's eye with the instrument's optical axis in such manner that the luminous device is positioned in the alignment axis with the eye. Such reflected image passes through axes A and B for reception, and the image is viewed through eyepiece lenses and/or screen (and/or observation device), respectively.

The invention, coupled to the Slit Lamp or an Ocular Microscope is composed of lenses, prisms, diaphragms and mirrors for focusing and receiving the reflected image, light signal emitters and receivers that emit and receive the reflection of the emitted signal, image sensors and a

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calculation system.

The instrument has two operational modes: the first mode measures corneal curvature radii in two orthogonal plans, while the second mode allows the measurement of corneal curvature radii in two non-orthogonal plans (bi-oblique astigmatism cases).

The two Slit Lamp eyepiece lenses are disposed on the alignment axis of the projection and imaging system.

The invention's **projection system** consists of a projected light ring onto the cornea in such manner that any distortion of the reflected image is analyzed for keratometric measurements.

The imaging system has an axis displaced from and substantially parallel to the aligning axis. This system deviates part of the image to the eyepieces of the slit lamp or ocular microscope and the other part to the image apparatus (or sensor) to be observed or displayed in a monitor, where both modes of operation of the instrument may be operated.

The calculation system consists in analyzing the deformation of the reflected image of the projected mire on the cornea, directly by observation or by computational methods, providing all parameters relatively to keratometry such as data and graphic interfaces of the examined cornea.

The invention, as claimed herein, especially developed for ophthalmic purposes, but with the possibility to measure curvature radii of any light reflecting surface, is composed of 5 fundamental parts: a) ring projection system; b) optics for viewing the examined eye; c) imaging system; d) control electronics; and e) mathematical and computerized system (images and data processing respectively), with the following scientific and construction concepts for industrial purposes.

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The first part of the invention is the light ring projection system, which consists of a mire that is attached to a slit lamp or ocular microscope in order to obtain the reflected image of the said mire reflecting means for displacing an image from said aligning axis to an imaging system axis and for returning said image to said aligning axis in an erect and unreversed position in order to provide both mire and corneal images in vertical and horizontal alignment with the cornea itself.

The Slit Lamp is an integrating part of the optics for viewing the examined eye and for the optical imaging system, through its eyepiece lenses, for the viewing of reflected image from the cornea which the ring was projected onto, allowing, through an optical set, that includes objective lenses and an optical assembly for corneal measurement, the image to be seen by the equipment's eyepiece lenses placed on the alignment axis at the opposite end of the light device in such manner that the first and the second axis coincide for viewing through the imaging sensor simultaneously or not with the eyepiece lenses.

The imaging system, through the optical system coupled where the two axes meet, implemented in the microscope has the purpose of sending a percentage of the image obtained by the microscope to its eyepiece lenses and to the video or computer screen.

With respect to the *invention's control electronics*, they are characterized by a sensor that indicates the eye being measured, left or right, and controlling the projection ring as well as the image receiving and pausing system.

Finally, the mathematical or computerized system, deals with image processing and consists of observation,

through direct or computerized methods, the reflected image from the cornea, distorted or not, and the *calculations*, which provides all keratometric data and data processing results of the cornea being examined.

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## STATE OF THE ART

For many years, optometrists, ophthalmologists and researchers of the ocular area have used equipment to study the eye. Some of this equipment has been in use simply to observe parts of the eye, subjectively, such as: magnifying glasses, Slit Lamps and bio-microscopes. Other instruments referred to as keratometers or ophthalmology meters have been used to measure the radii of corneal curvature along the two main meridians of the eye. The functioning principle of such instruments is already well known, as shown by several chapters in books such as "The eye and Visual Optical Instruments" published in 1941 by Smith George and Atchison David A. Cambridge University Press, p.175.

Currently, keratometers already carry technological advancements that allow the measuring of corneal curvature radii, some equipped with ring projection covering the entire surface, showing the topography of the cornea.

All of them have their own optics, some automated, but presenting high manufacturing costs for separate and exclusive optics for this kind of measuring.

The existing non-automated keratometers, besides giving a relatively broad scale of measure background, do not allow for non-orthogonal axes measurements (only orthogonal), possible only by automated equipment, greater part of which do not have measurement interval that is broad enough, in addition to extremely high cost.

For better understanding and to show evidence of

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the invention's innovations, assisted through the drawings attached herein and illustrating the present request or patent, a detailed description of the keratometric module's frame is presented – figure 1-, constructed for coupling to instrument (1) - Slit Lamp or Microscope - with a projection illuminated ring (2) - figure 2 - coupled to the objective lens or any fore part of the Slit Lamp (1), on projection axis A. Between the projection axis and reception axis A and the eyepiece lenses is inserted a system (3) for partial beam deviation to axis B, which is composed by prisms and/or semi-transparent mirror that deviates the reflected image of the ring's projection (2) onto the eye of the positioned patient (7) in axis A to the eyepiece lenses (8) of the instrument (1) and to axis B, at the imaging sensor (4) and further on to the observation apparatus (6) - video screen. The ring (2) is focused onto the patient's eye in position (7) by the joystick (9) of the instrument (1), which allows moving it in directions X, Y and Z of the Cartesian plane, and observed in real time in positions (8) and (6). The eye sensor (5), figure 3, placed in one of the instrument's (1) ends along axis C, has light signal emitters and receivers (5a) and (5b), and a hole for power supply cable. controlled by the microcomputer as shown in figure 3. The emitter (5a) emits a signal that reaches the instrument's assembly (1), which, if positioned in the same end as the emitter (5a) along axis C, reflects the signal transmitted by the emitter (5a), being received by the sensor (5b) whose reception indicates the instrument's (1) position and thus indicates the eye (7a), as shown by figure 2, being measured.

Absence of signal (5b), signal not reflected by instrument (1), indicates that the opposite eye is the one being measured.

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To project a light ring (2) with the necessary luminosity on the patient's eye, a light ring or illuminated ring (2) is provided.

The light ring (2), better seen in figure 2, is opaque of and has a central circular hole (11) with a light source, flashing or not, and two holes (12a and 12b) so that observation through the two Slit Lamp (1) eyepiece lenses is not blocked. There are several holes (13) placed in precise circular shape on the ring (2a), more than 5 in number, around the central hole (11). Several light sources (13a) are inserted into the holes (13), a source for each hole.

When the lights (13a) are activated, the light from these holes reach the patient's cornea (see figure 4) and project an image right behind the one reflected by a patient's eye (7a), the same occurring for the other eye (7b) when the equipment is positioned to examine it.

This reflected light is the image that goes though the instrument (1) under its measurement mode.

The apparatus for viewing the image is composed 20- by a video sensor (4), information forwarding system to microcomputer (frame grabbers – boards or cable) (4a) and microcomputer screen (6) coupled to a microcomputer. Alternatively, the ring (2) may be like the other ring (2b) with an illuminated or luminous ring in precisely continuous circular shape.

As seen in figures 1 to 4, an imaging system (3), (4), (4a) and (6) is placed along axis B coupled to the instrument (1) on its axis A.

The system uses the objective lens and image enhancing drum of the instrument (1) to optically obtain the image reflected by the patient's eye while the distorted or

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non-distorted reflection of the ring's projection (2) of a circular figure on the patient's eye is obtained and analyzed by a microcomputer. The distortion (deviation of the circularity) of reflected image of the projected light mire target is analyzed, and the dimension of the said image and quantity of distortion provides data for determining the radii of curvature (or refractive power) along the 360°, as well as the major and minor radii of curvature of the surface (or refractive power), which can be obtained in both modes of measurement (orthogonal or non-orthogonal).

Keratometry analysis is thus obtained.

Figure 1, which accompanies and illustrates the invention shows the side view of the entire system of the present invention coupled to a Slit Lamp (A, B and C axes).

Figure 2 presents the invention in frontal view for coupling to the present invention's system along axes A-B of figure 1.

Figure 3 shows a topographic view of the frame, light signal emitters and receivers of the eye sensor used in the invention.

Finally, figure 4 shows the upper View of the ophthalmologic instrument developed for instrument 1, of ring projection 2 on the eyes 7a and 7b of the patient.

As known, an innovative process must incorporate industrial features and applications to satisfy cost/benefit needs of professionals of the area and patients, and stand out in the market.

The present invention has such requisites, with principles and singular characteristics, and which innovative method has proved fully efficient in its constitution and application according to the descriptive report. In view of such

advantages, and the technical impact created, the present object gathers the necessary conditions to entitle it the privilege claimed.